Particle Separation Using Deterministic Lateral Displacement

# **Design Objective**

- Design a microfluidic device capable of separating particles of varying sizes
- Should be small
- Easy to fabricate
- Durable for multiple usage and possible high throughput applications



### 1. Hydrodynamic Chromatography PROS

- Efficient with high sensitivity
- No sample loss
- Well defined separation times <u>CONS</u>
- Multipath effect reduces resolution
- High diffusion effect
- Large scale set up



http://www.chemistry.adelaide.edu.au/external/soc-rel/content/size-exc.htm



### 2. mAECT- mini Anion Exchange Centrifugation Technique

### <u>PROS</u>

- high selectivity, detection limit ~ 100 trypnasomes /ml
- Works on charge difference in cells

### <u>CONS</u>

- Large scale experiment set up.
- Difficulty to view under microscope.
- Requires pre-treatment to increase concentration of trypnasome





3. Cell lyses

#### <u>PROS</u> –

- Simple and fast method of concentration RBC.
- Detection limit of ~ 500 trypnasomes/ml blood.
- Sensitivity increased by 20%

#### <u>CONS</u>-

 Pretreatment, Centrifugation of blood required before detection.



The sediment at the bottom contains both parasites and white blood cells

The only one-step, closed system for collection, cell separation and transport.

For the Separation of Mononuclear Cells from Whole Blood.



- There are several on-chip methods used, but they all have limitations.
  - Physical features are easy to implement but are very limited.



- Dielectrophoresis
- Magnetic
- Deterministic lateral displacement

## Theory

- Deterministic lateral displacement
  - Works by using the mechanism of laminar flow past an array of posts.
  - The array of posts divide the flow into several different streams.
    - Since the flow is very low Reynolds number there is very little diffusion and mixing between streams.
    - If the particle is smaller than the stream, it will travel within it.
    - If the particle is larger than the stream, it will pushed laterally by the posts.



### Theory



### Theory

• The size of particle to be separated (critical diameter) is dependent on 3 variables.

- The diameter of the posts
- The distance between the posts
- The offset of the posts

• The following equations can be used to estimate the size of the particles that will be separated.

$$D_{c,n} = 1.4 dN_n^{-0.48}$$
$$N_n = \lambda / \Delta \lambda_n$$
$$d = \lambda - D_{post}$$



### **Determination of Design Parameters**

Section	Row Shift	Critical Diameter
	μm	μm
1	0.8	3.95
2	1.6	5.52
3	2.6	6.97
4	3.8	8.36
5	5.2	9.72
6	6.8	11.06
7	8.8	12.52

- Posts are 50µm in diameter, and have 25µm spacing.
- Using the previous equations we designed our system to have 7 sections, each capable of separating different sized particles.
- The smallest size particle our system can separate is theoretically 4µm

# Apparatus

### Utilized AutoCAD to create mask design





# Fabrication

#### <u>Master Mold</u>

- SU-8 photoresist, 30 µm thickness
- Spin speed 3,000 rpm for 2025 resist
- UV lamp energy 2 mJ/cm
- Exposure time was 75 seconds

#### • <u>PDMS</u>

- 10:1 PDMS to curing agent ratio
- 3 mm thick

### Glass Substrate



### **Final Device**

- Initial fabrication resulted in a device with no posts causing the main chamber to collapse
- The second fabrication used more sensitive photolithography equipment and resulted in better definition of the posts



### **Final Device**



#### Fabrication 1

Fabrication 2

### **Final Device**

 The post size came out to ~55 µm within 10% of our original design parameters



### Experimental Set-up

- Testing the separation between two different particle sizes, 2.8µm and 15µm
- Flow induced by syringe pump and varied between 2 and 200 µL/min
- Both beads were first pushed through the device separately to observe any possible flow patterns

### Results

- Small beads were too small to record their flow on video
- Most of the particles aggregated around posts near the inlet even though some did reach the correct outlet well



# Results

- Were able to inject large beads but flow was inhibited
- Several beads moved to the outlet but the majority were stuck near the inlet



#### <u>Lithography</u>

- Our design was very sensitive to any lithography limitations.
- Mask
  - Rough edges on the mask led to imperfect circles
- Exposure
  - Over exposure could lead to no or non-uniform posts
- <u>PDMS</u>
  - Small post diameters led to some breaking off in master mold



Post diameter varied from 55µm at PDMS surface to 33µm at glass surface



- Areas where we left out partial posts became traps for beads.
- Beads stuck to posts.
  - Could be cause by surface roughness of posts



- Dust particles obstructed flow patterns forcing beads to aggregate
- Larger particles also adhered to the posts

## Conclusions

- Posts for the second fabrication were more defined due to more accurate photolithography process
- Lifetime of device was limited due to outside contamination
- Were able to determine bead flow in the device but couldn't demonstrate proper separation

## Future Work / Recommendations

- More sensitive photolithography will lead to more uniform posts
- Treatment of PDMS beforehand to minimize particle adhesion and aggregation
- Operation under a hood or in a clean room would be ideal to limit contamination
- Modify design to allow ample space for microscope to view inlet flow of particles

## Future Work / Recommendations

- After testing lateral displacement for particle sizes, design appropriate outlet spacing
- Possible addition of antibody ligands to better capture and sort particles in each flow stream



### QUESTIONS?



# References

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